

Modelovanie elektrickej aktivity srdca v prostredí COMSOL Multiphysics

**(Modeling of the electrical activity of the heart
in COMSOL Multiphysics environment)**

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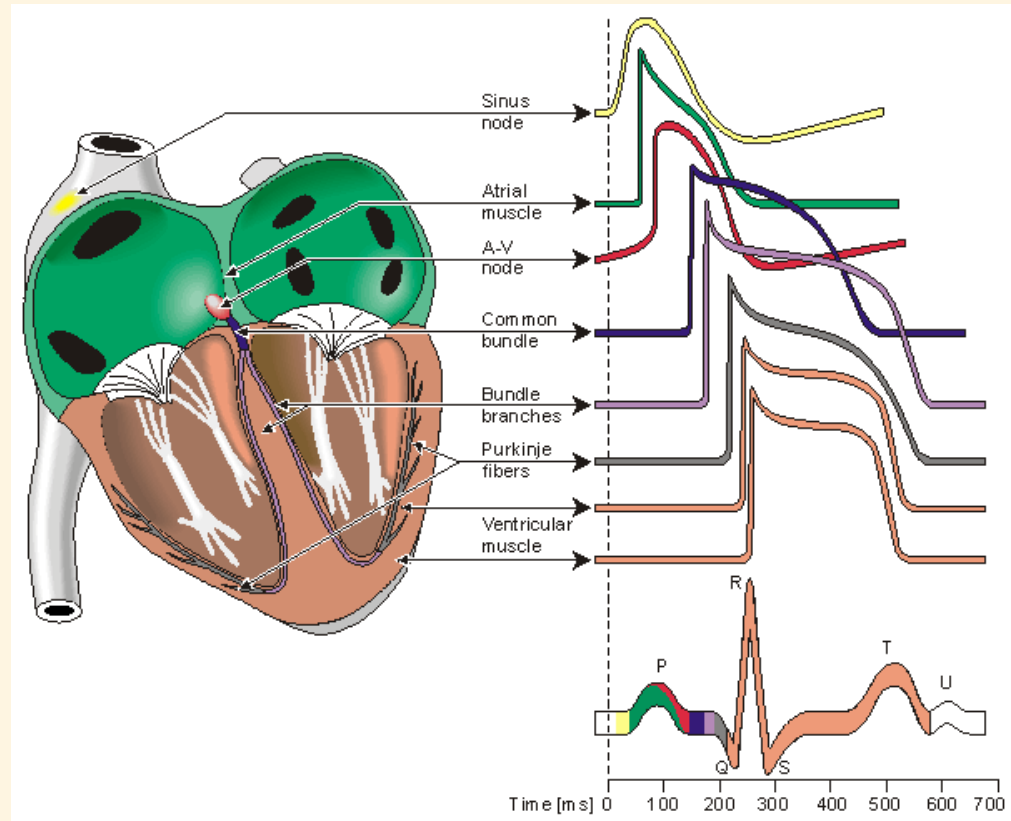
PRESENTATION OUTLINE

- **Electrical excitation - action potential (AP) in the heart**
- **Models of AP of atrial and ventricular heart cells**
- **Simplified model of heart cells (modified FitzHugh-Nagumo model) – in Matlab**
- **Modeling of AP propagation – monodomain model**
- **Modeling of AP propagation - in COMSOL Multiphysics**

Electrical excitation of the heart

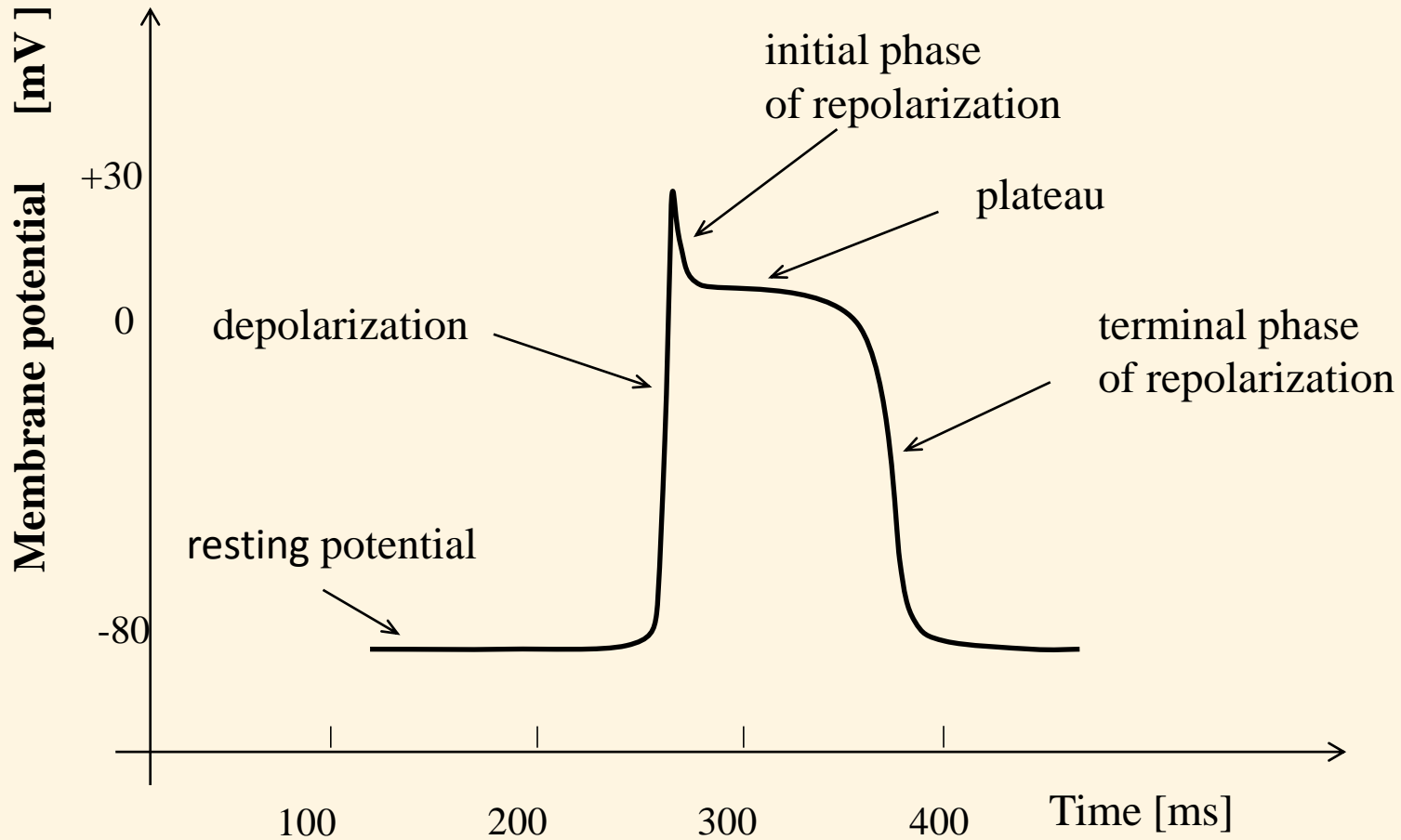
Electrical excitation (in form of action potential) is spreading in the heart through various types of heart cells [1] – [3]:

- **SA nodal** – origin of excitation
- **Atrial**
- **AV nodal**
- **Bundle of His**
- **Bundle branches**
- **Purkinje fibers**
- **Endocardial**
- **Mid-myocardial**
- **Epicardial**



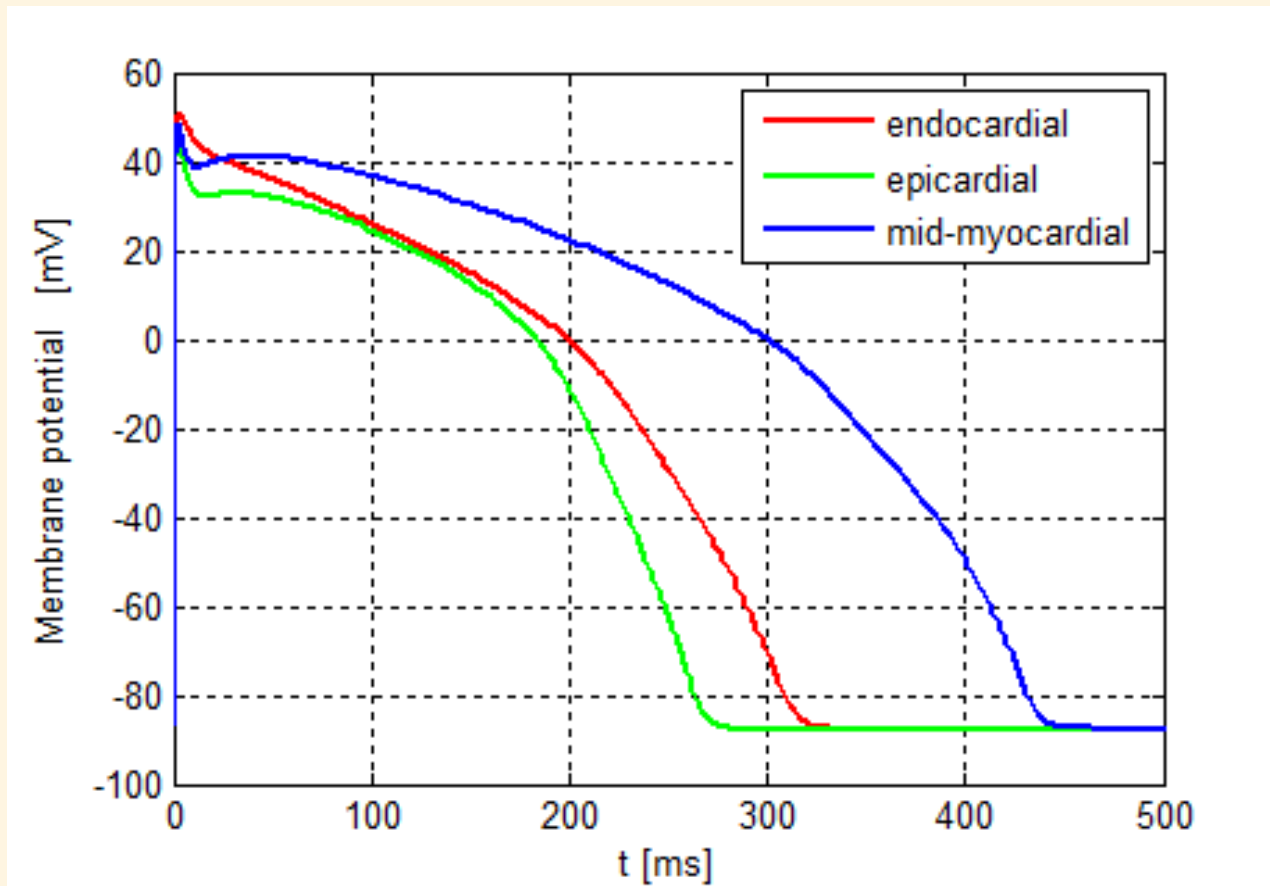
Action potential shape [2] is different for different types of heart cells

Action potential



Action potential phases in typical cardiomyocyte (cardiac muscle cell)

Various types of cardiomyocyte action potential shapes



Various types of action potential shapes in ventricular cardiomyocyte [4], [5]

Models of heart ventricular cells [4] – [11]

Luo – Rudy I model (1991) [6]

Luo – Rudy II model (1994) [7]

Winslow model (1999) [8]

Shannon-Bers model (2004) [9]

Hund-Rudy dynamic model (2004) [130]

O'Hara-Rudy model (2011) - enables to model [4], [5]:

- epicardial
- endocardial
- mid-myocardial cells

Model of heart atrial cells [12] - [15]

Courtemanche-Ramirez-Nattel model (1998) [12], [13]

enables to control AP morphology (three main morphological types)
- 21 ordinary differential equations (ODE)

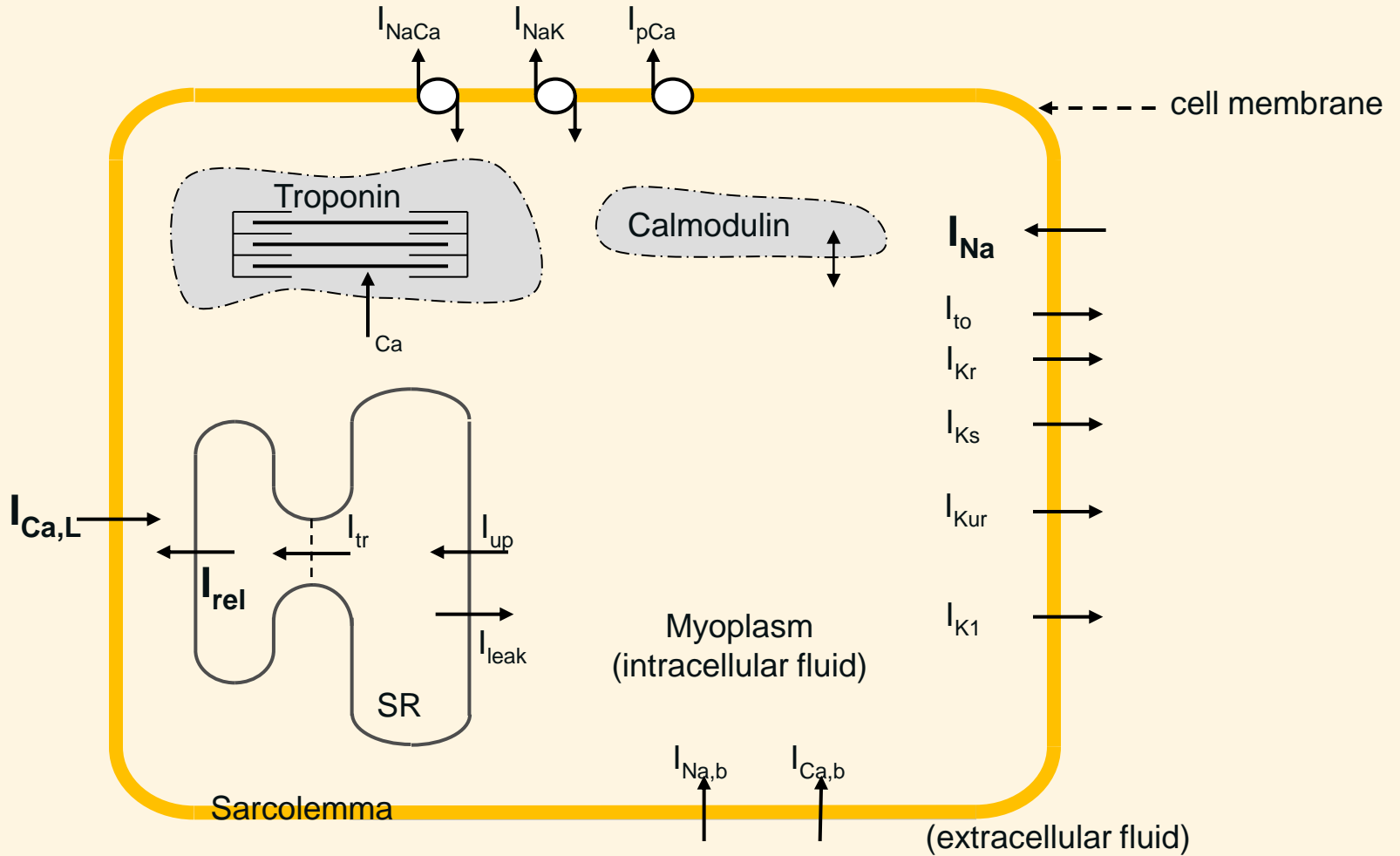
Simplified model of heart cells

modified FitzHugh-Nagumo model [16] – [20]

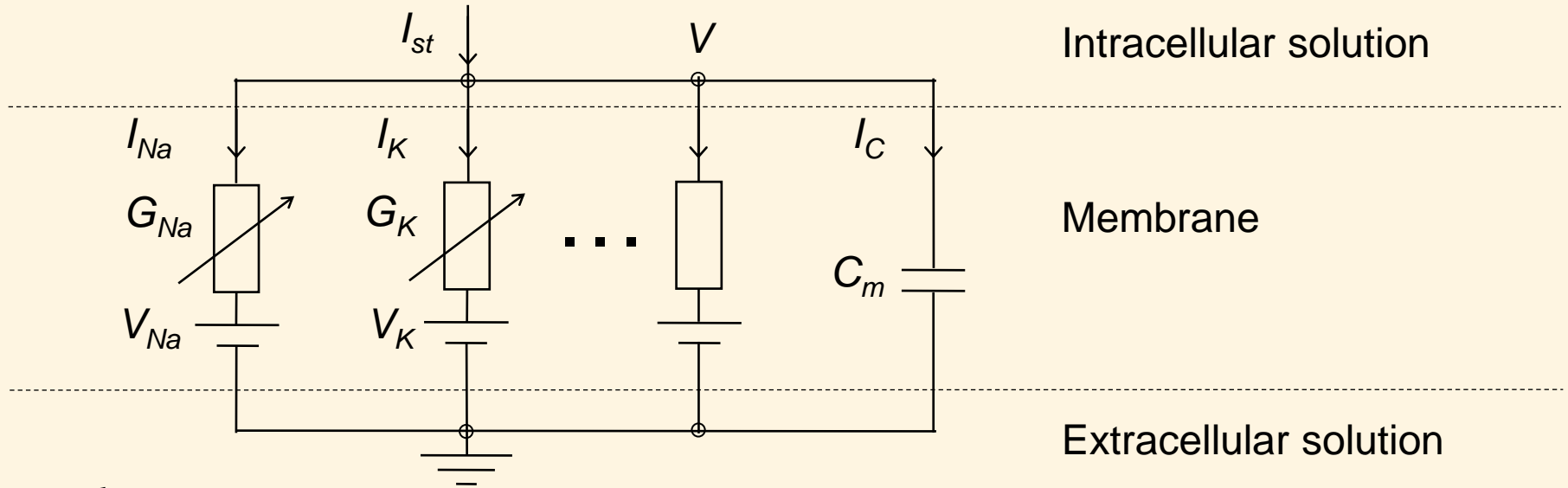
enables to control AP shape

- 2 ordinary differential equations

Courtemanche-Ramirez-Nattel model of human atrial cell [12]



Courtemanche-Ramirez-Nattel membrane model of the human atrial cell



$$\frac{dV}{dt} \cdot C_m + I_{ion} = I_{st} \quad \Rightarrow \quad dV/dt = (-I_{ion} + I_{st})/C_m$$

$$I_{ion} = I_{Na} + I_{Ca,L} + I_{to} + I_{Kr} + I_{Ks} + I_{K1} + I_{Kur} + I_{NaK} + I_{NaCa} + I_{Ca,p} + I_{Ca,b} + I_{Na,b}$$

where e. g.:

$$I_{Na} = G_{Na} m^3 h (V - V_{Na})$$

21 ordinary differential equations (ODE)
75 algebraic equations

Modified FitzHugh-Nagumo model of the cardiac cell

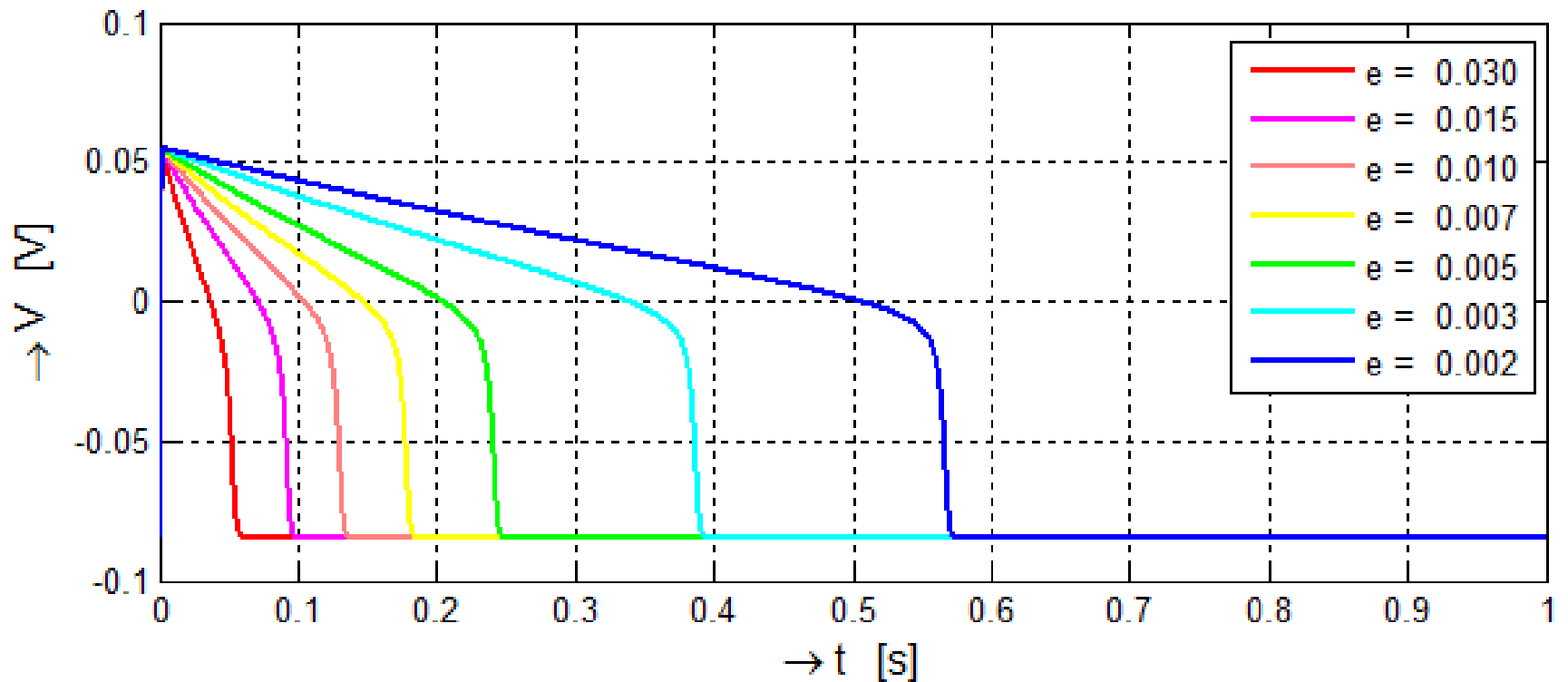
- using **modified FitzHugh-Nagumo** equations [16] – [20]

$$\frac{dV}{dt} = -k c_1 (V_m - B) \left(-\frac{(V_m - B)}{A} + a \right) \left(-\frac{(V_m - B)}{A} + 1 \right) - k c_2 R (V_m - B)$$
$$\frac{dR}{dt} = k e \left(\frac{(V_m - B)}{A} - R \right)$$

where V_m is the membrane potential,
 R is the recovery variable
 a is relating to the excitation threshold
 e is relating to the excitability
 A is the action potential amplitude
 B is the resting membrane potential and
 c_1 , c_2 , and k are membrane-specific parameters.

FitzHugh-Nagumo model – simulation in Matlab

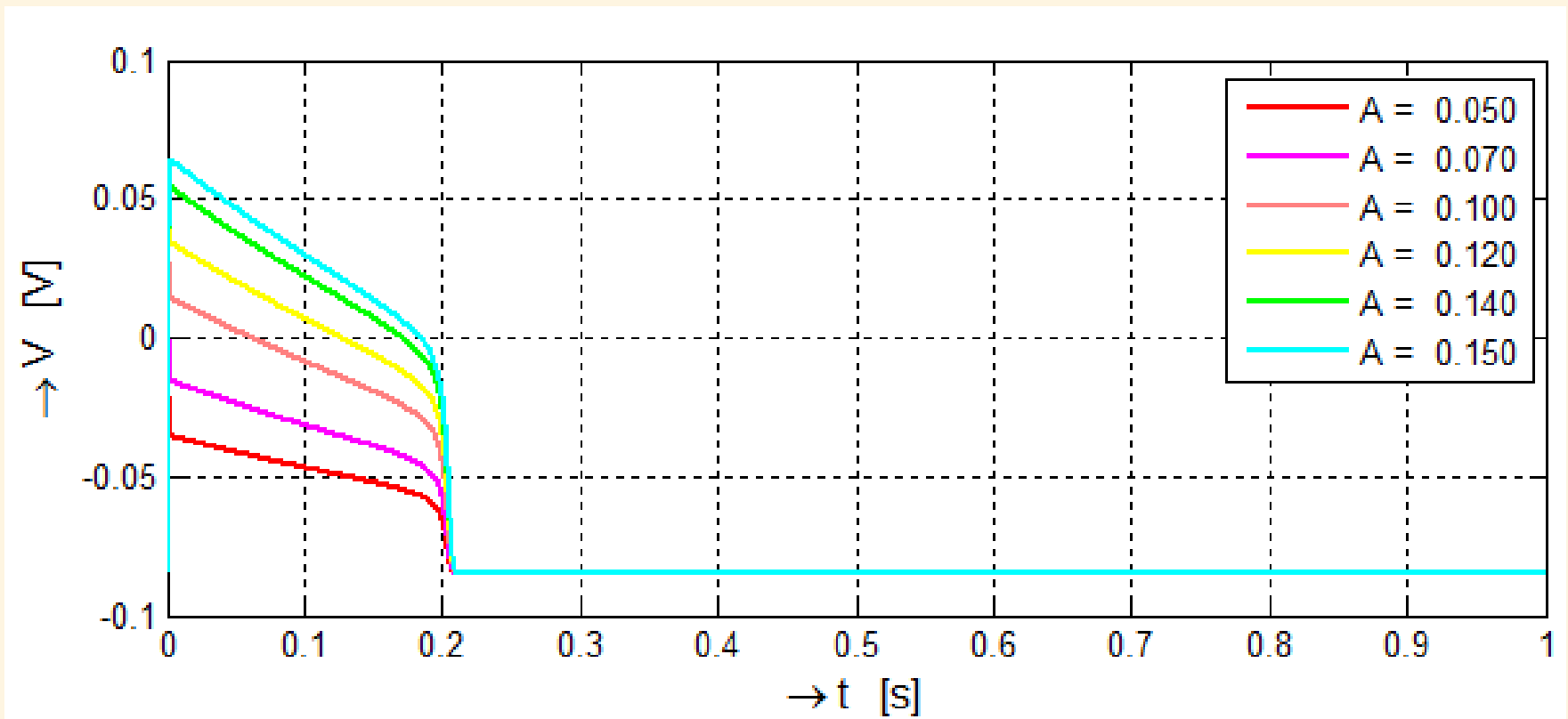
Influence of membrane parameters on :
- action potential duration (APD)



Influence of membrane parameter "e" on APD [20].

FitzHugh-Nagumo model – simulation in Matlab

Influence of membrane parameters on :
- action potential amplitude (APA)



Influence of membrane parameter “A” on AP amplitude [20].

Modeling of propagation of electrical activation using monodomain model

- monodomain model [21], [22] with incorporated modified FitzHugh-Nagumo equations [18] – [20], [23]

$$\frac{\partial V_m}{\partial t} = \frac{1}{\beta C_m} \left\{ \nabla \cdot (\sigma \nabla V_m) - \beta (I_{ion} - I_s) \right\} \quad D = \frac{\sigma}{\beta C_m}$$

where

V_m is the membrane potential,

β is the membrane surface-to-volume ratio,

C_m is the membrane capacitance per unit area,

σ is the tissue conductivity,

I_{ion} is the ionic transmembrane current density per unit area and

I_s is the stimulation current density per unit area. 13

Simulation parameters

- of monodomain model with modified FitzHugh-Nagumo equations:

$a = 0.13$ - relating to the excitation threshold

$e = 0.0132$ - relating to the excitability

$A = 0.120 \text{ V}$ - the action potential amplitude

$B = -0.085 \text{ V}$ - the resting membrane potential

$c_1 = 2.6$ - membrane-specific parameter

$c_2 = 1$ - membrane-specific parameter

$k = 1000 \text{ s}^{-1}$ - membrane-specific parameter

$D = 0.0005 \text{ m}^2/\text{s}$ - diffusivity

.

Modeling of propagation of electrical activation in COMSOL Multiphysics

- monodomain model for AP propagation in the heart is:

$$\frac{\partial V_m}{\partial t} = \frac{1}{\beta C_m} \left\{ \nabla \cdot (\sigma \nabla V_m) - \beta (I_{ion} - I_s) \right\}$$

- this PDE (partial differential equation) is numerically solved in COMSOL Multiphysics
- detailed description how realize similar example for heart of ellipsoidal shape in COMSOL Multiphysics is in [23]:

Select Physics:

→ Δu Mathematics

→ Δu PDE Interfaces

→ Δu General Form PDE (g)

Modeling in COMSOL Multiphysics

General Form PDE (g)
in COMSOL Multiphysics:

Equation

Show equation assuming:

Study 1, Time Dependent

$$e_a \frac{\partial^2 \mathbf{u}}{\partial t^2} + d_a \frac{\partial \mathbf{u}}{\partial t} + \nabla \cdot \Gamma = f$$

where: $u \rightarrow V_m$

$$e_a = 0$$

$$d_a = 1$$

Mathematical description of
monodomain model:

$$\frac{\partial V_m}{\partial t} = \underbrace{\nabla \cdot \left(\frac{1}{\beta C_m} \sigma \nabla V_m \right)}_{-\Gamma} - \underbrace{\frac{1}{C_m} (I_{ion} - I_s)}_f$$
$$i_{ion} = \frac{I_{ion}}{C_m}$$

Modeling geometry of heart wall

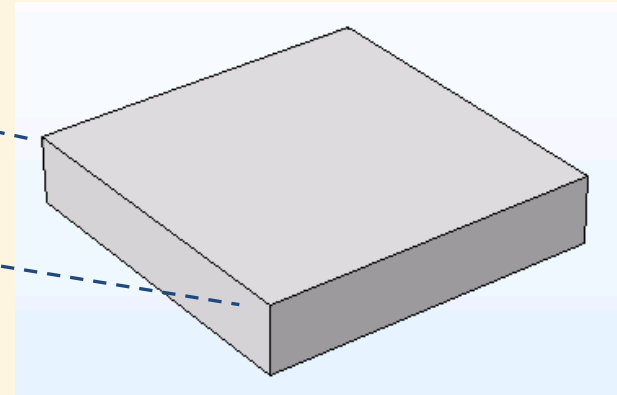
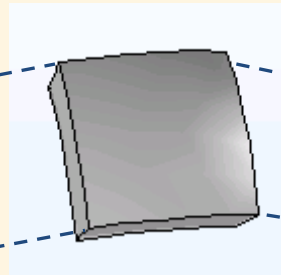
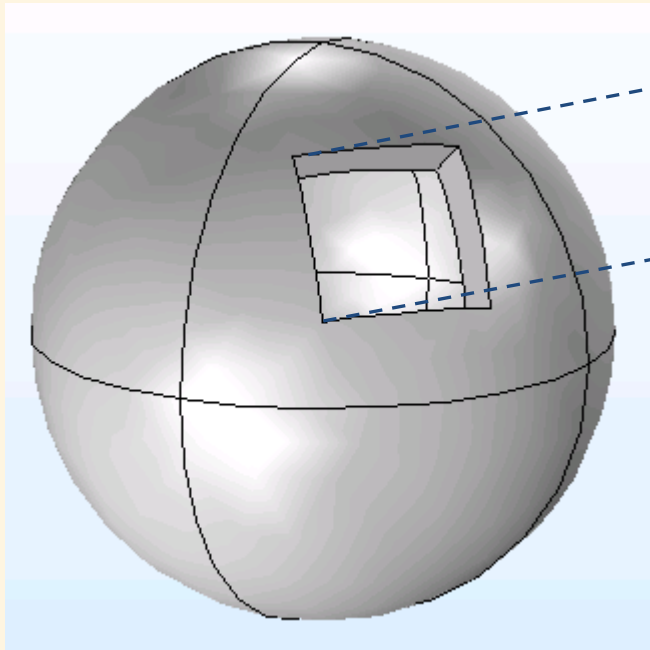
whole heart as a hollow sphere:



part of heart wall:

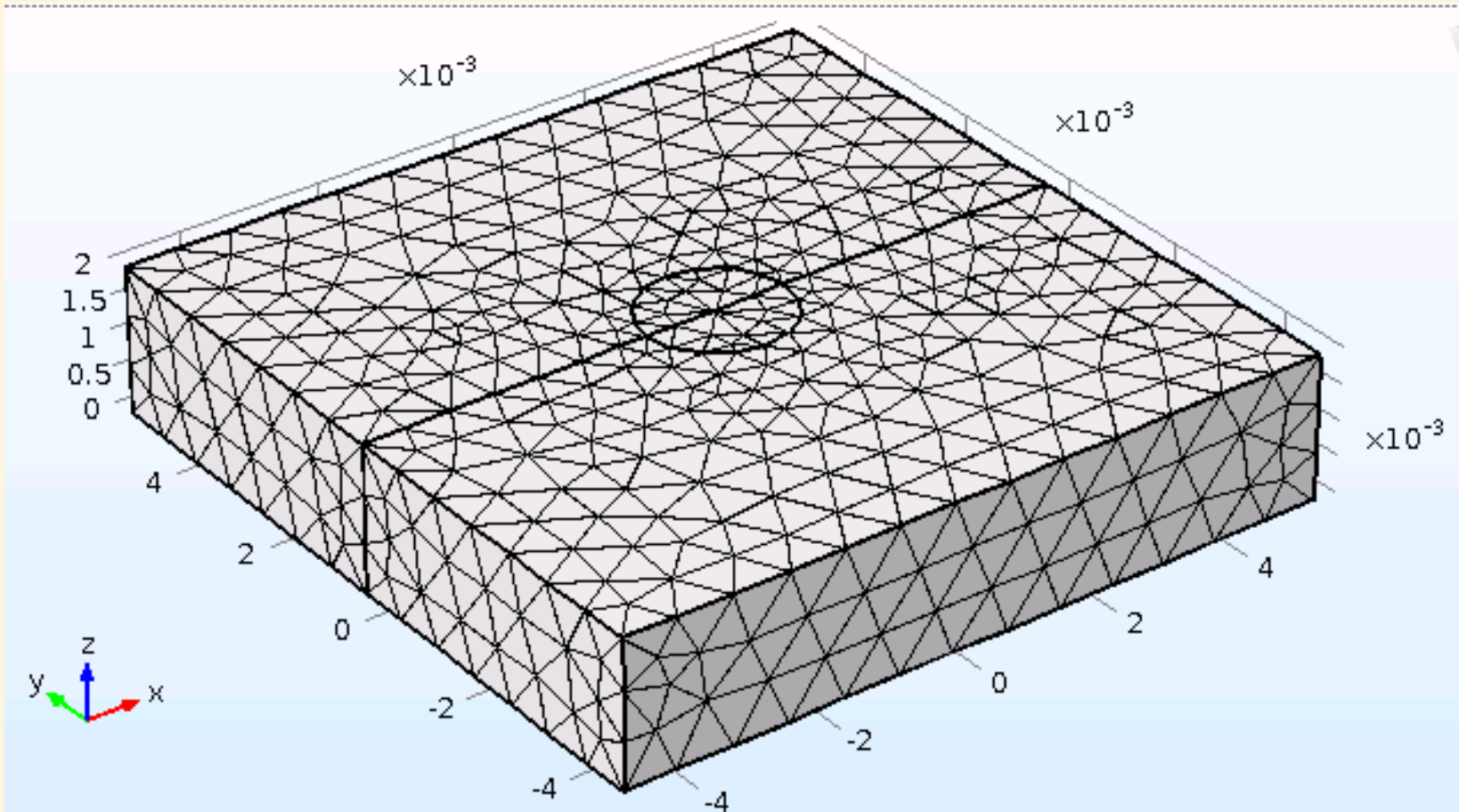


approximate part of heart wall of box (“SLAB”) shape:



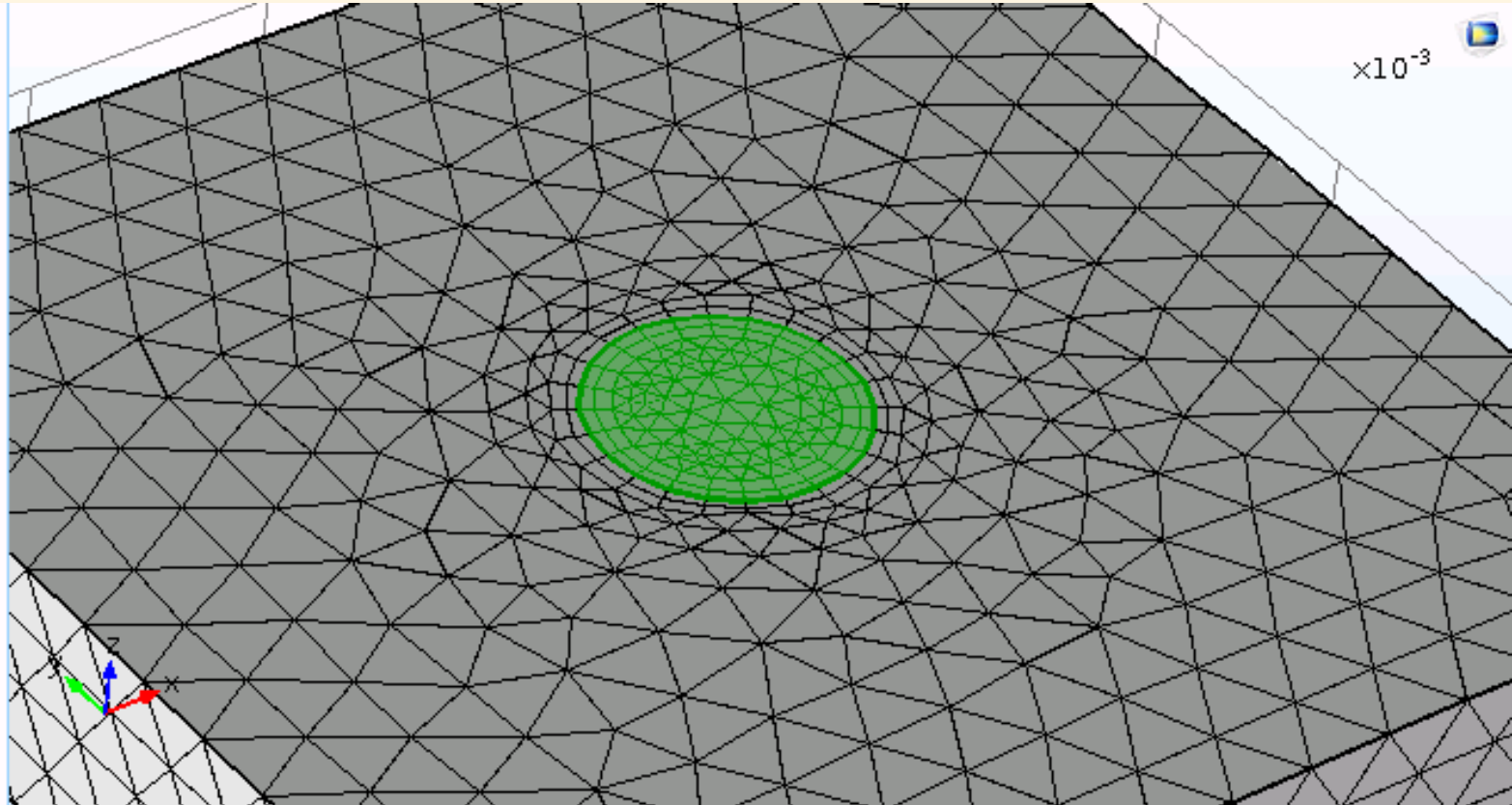
the SLAB model of wall that is used for the following simulation

Meshing of the model



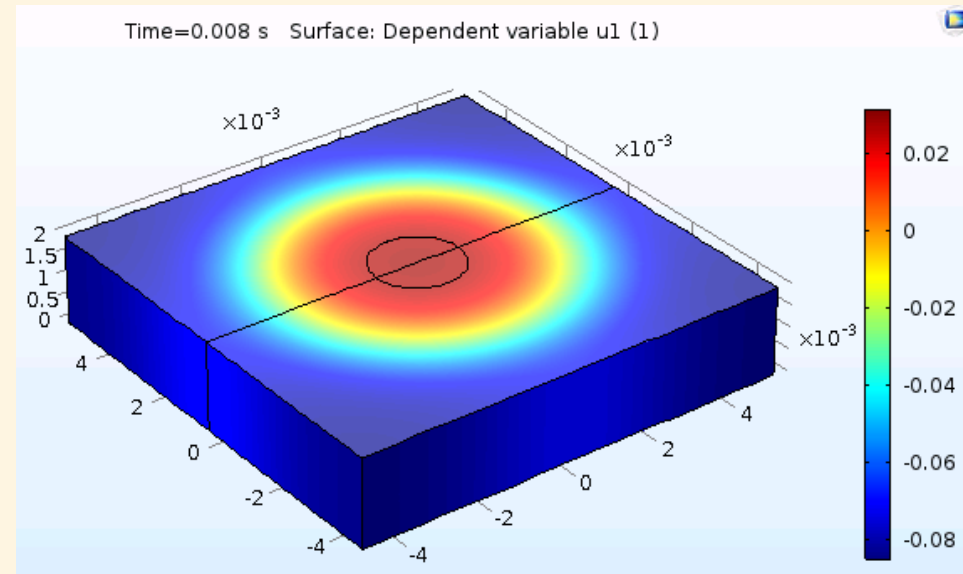
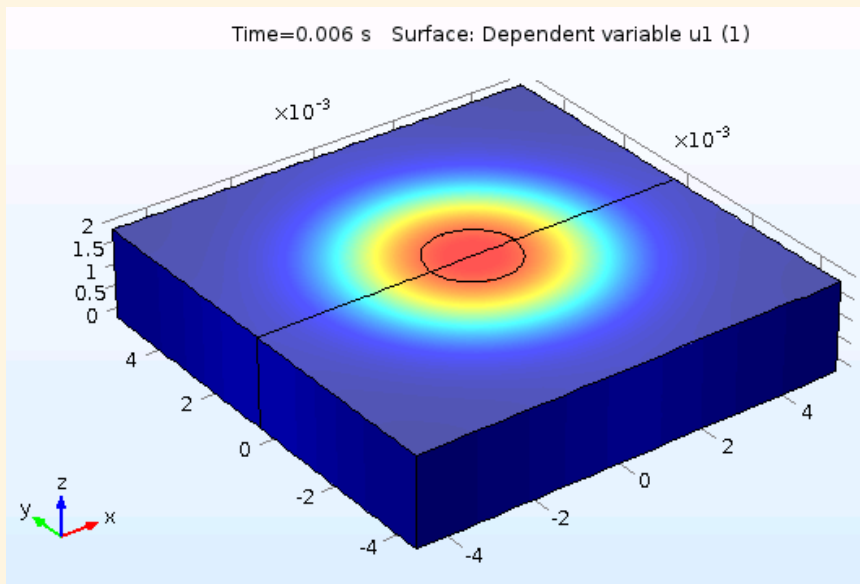
The SLAB model of the heart wall covered with mesh (predefined „Fine“ mesh). The stimulated area is a cylinder with $r = 1$ mm radius situated in the middle of the slab model.

Meshing of the model



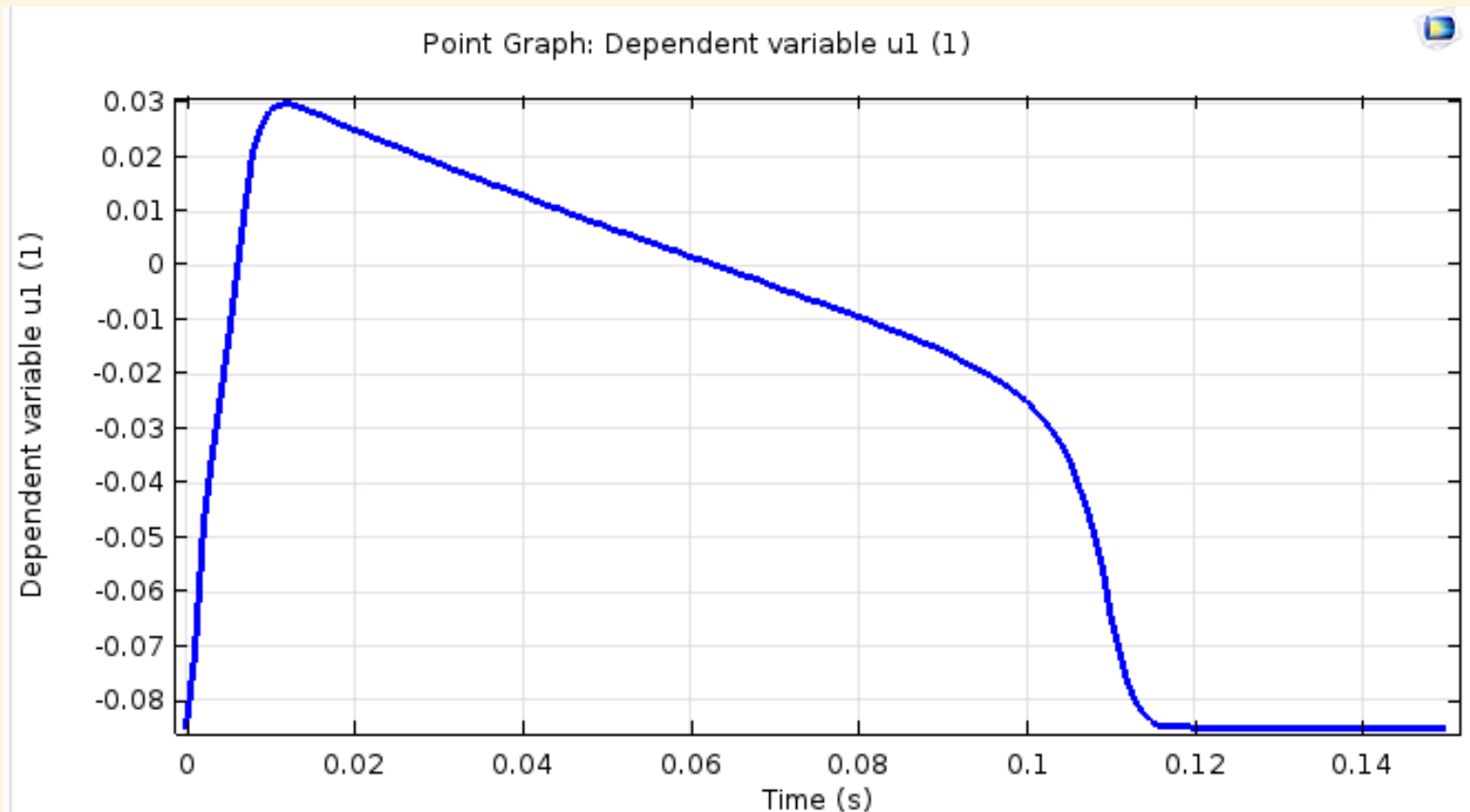
More dense meshing of the SLAB near the boundary of stimulated area of $r = 1$ mm radius (green) is performed with two manually added boundary mesh layers from both sides.

Propagation of AP – simulation results



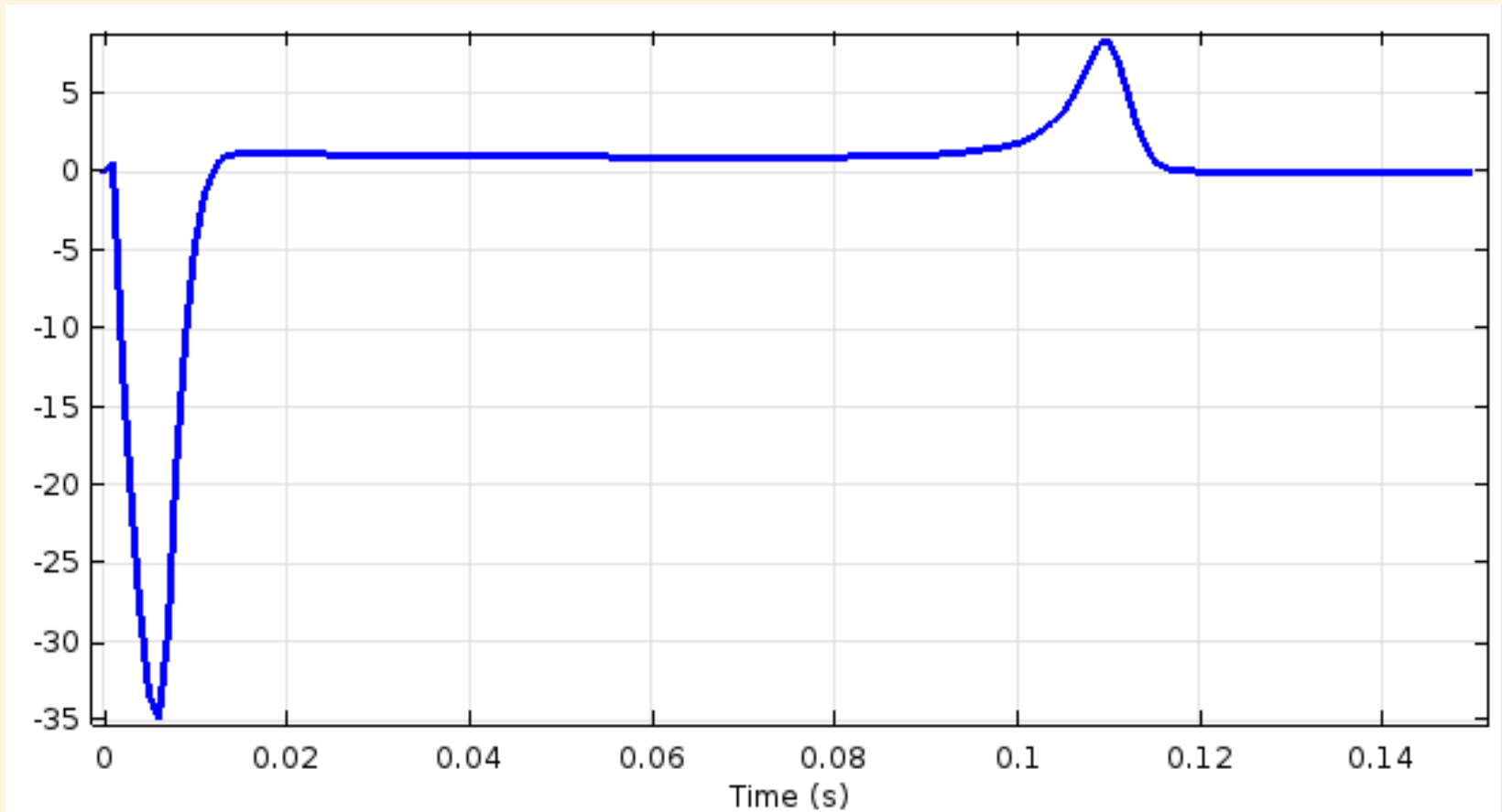
Distribution of membrane potential [V] in the SLAB model at 0.006 s and 0.008 s after stimulation onset ($r = 1$ mm, stimulation duration $T_s = 0.002$ s, amplitude of stimulation current $i_s = 100$ A/F). Activated area is shown in red, resting area in blue.

Action potential in Point Probe



Distribution of membrane potential [V] (action potential) in the slab model in point $x = 1.5$ mm, $y = 0$ mm, $z = 2$ mm ($T_s = 0.002$ s, $i_s = 100$ A/F).

Ion current in Point Probe



Distribution of I_{ion} normalized current [A/F] in the slab model in point $x = 1.5$ mm, $y = 0$ mm, $z = 2$ mm ($T_s = 0.002$ s, $i_s = 100$ A/F). First negative current causes depolarization of membrane (AP onset), positive peak of current causes membrane repolarization (terminal phase of repolarization).

Conclusion

Simulation of electrical activity (AP) of heart cell using FitzHugh-Nagumo equations

- ordinary differential equations (ODE)
- in Matlab.

Simulation of **AP propagation** in heart tissue using monodomain model with FitzHugh-Nagumo equations

- partial differential equations (PDE)
- in **Comsol Multiphysics**.

THANK YOU FOR YOUR ATTENTION!

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